OPTIMIZING A WHEELCHAIR

Taking Advantage of the Technology to Get Best Outcomes, Now and In the Future

PRESENTED BY

Tom Whelan V. P. Product Development



MANUAL WHEELCHAIRS: THE SCIENCE THAT SHOULD BE DRIVING YOUR CLINICAL CHOICES

This Presentation is Part of a Series

How Do People Actually Use Their Manual Wheelchairs, and What Really Matters?

The Impact of Wheels and Tires on Wheelchair Propulsion Efficiency

Optimizing a Wheelchair: Using the Technology to Ensure Ongoing Success

3

Manual Wheelchairs How Do People Actually Use Their Manual Wheelchairs and What Really Matters? Ki_Mobility



Why are we tackling this subject matter?

A Wheelchair is a Machine

It provides a mechanical advantage to make mobility easier





The wheelchair as a machine has an inherent mechanical efficiency

 There is nothing that the user, *in the* act of propelling it, can do to improve it

Ki/



What can be done to affect the inherent efficiency of this machine?

Ki∠

- Wheelbase Adjustment
- Wheel and Tire selection
- Seating Adjustment



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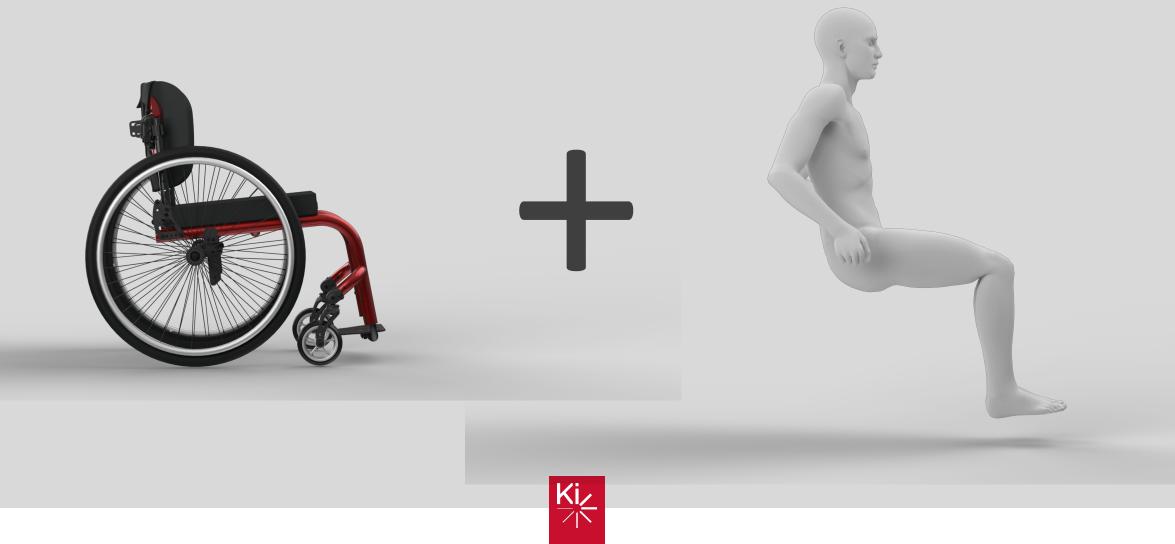
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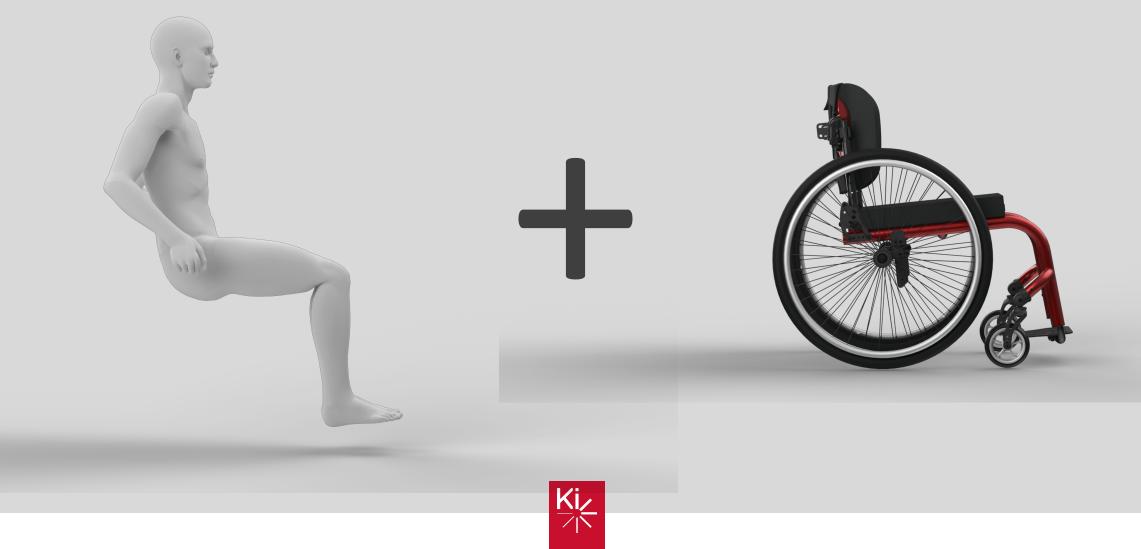


The Two Components of Propelling a Wheelchair





The Two Components of Propelling a Wheelchair



Dissatisfaction and Abandonment of Wheelchairs

Dissatisfaction with, abandonment of, mobility equipment is high

Why?

- Lack of user opinion in selection (Phillips & Zhao, 2010)
- Improper fit to the user and to tasks the user wishes to undertake (Scherer & Galvin, 1996)
- Myth that "a user's assistive technology requirements need to be assessed just once" (Scherer & Galvin, 1996)

What can we do to address it?

Wheelchair ['(h)wel_CHer]

NOUN

a chair fitted with wheels for use as a means of transport by a person who is unable to walk as a result of illness, injury, or disability.

A type of mobility device for personal transport

(Taber, 2005)





findawi Publishing Corporation Rehabilitation Research and Practice Wohume 2012, Article ID 753165, 7 pages ot:10.1155/2012/753165

Research Article

Manual Wheelchair Use: Bouts of Mobility in Everyday Life

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Background. This study aimed to docribe how people move about in manual wheekhairs (MWCa) during everyday life by evaluating bouts of mobility or continuous periods of movement. Merkods. A convenience sample of 28 MWC users was recruited. evaluaring bouts or moonly or commuous persons or movement. Atendes: A convertience sample of 28 MWC users was recruited. Participants' veryday mobility was measured using a wheel-mounted accelerometer and sent company which for 1.2 weeks. Bouts of mobility many mounted and characterized and characterized and the same the motion bound and all commit Paracipanse everycay monitity was measured using a whees-mounted accelerometer and seat occupancy switch for 1-2 weeks. Bout of mobility were recorded and characterized. Results. Across 29,000 bouts, the median bout lasted 21 seconds and traveled houss or monenty were recorded and characterized. Action Action Actions for forman down and the statement of 6.6 m at 0.45 m/s. 80% of recorded boats tasted less than 1 minute and traveled less than 30 meters, Farbicipants: dairy wheeknar activity included 90 boats and 1.6 km over 54 minutes. Average dairy occupancy time was 11 hours during which participants activity included 90 boats and 1.6 km over 54 minutes. Average dairy occupancy time was 11 hours during which participants activity moases to south and Loam over 54 minutes. Average casy occupancy time was 11 hours during which participants wheeled 10 loukulour and append 10% of their time wheeling. Spearman-Bown Prophecy analysis suggested that 7 days sere sufficient to achieve a reliability of 0.8 for all boat variables. Cardinations. Short, slow louis dominate wheelchair sange in a summers to science a reparative or too for an over variators. Concusions, soor, now pouse commare wheeschair usage natural environment. Therefore, clinical evaluations and biomechanical research should reflect this by concentrating on initi hauma environmente. Loterorie, camcai evaluations and momentanical research snouid retiect insi by concentrating on initiating movement, maneuvering whetchairs, and stopping. Bouts of mobility provide greater depth to our understanding of whetchair use and are a more stable metric (day-to-day) than distance or time wheeled.

1. Introduction

The study of activity has been of interest for many years as a means to relate activity and health outcomes. The study of activity specifically among persons with disabilities has garnered recent interest with respect to health and community participation [1, 2]. Decreased mobility can impact health status and has been associated with issues such as diabetes

As a means to characterize activity, research has documented how far people walk datly [7-9], and guidelines have been developed to establish goals or metrics for walking activity [10, 11]. Bohannon synthesized published data and documented stmtlar walking activity across gender, and differences across certain geographic regions [12]. Further-more, he found that most studies reported that adults, especially older adults, in the United States walked fewer than

Analogous data has also been collected on manual wheel-

chair mobility with authors reporting the distance traveled week-tair mobility with authors reporting the distance traveled

spent moving and average speed [13-17]. Table 1 lists the results of five such studies. Despite diverse subject groupings, the datly distance results are fatrly similar with the exception of a study using competing athletes, Other research into mobility considered how people move

as opposed to how far people move. Bouts of mobility, or continuous segments of movement, have been reported as a means to describe ambulation and wheelchair movement [6-8, 18, 19]. In ambulation studies, steps taken over short epochs of time are reported as a means to describe walking patterns [6, 7]. Results indicated that people overwhelmingly walk in short bursts. Levine reported that 97% of ambulation bouts lasted less than 200 seconds, and Orendurif et al. reported 90% lasted less than 100 steps.

Bouts of wheelchair mobility have been measured and reported for power wheelchair users [19]. When applying this construct to wheeled mobility, bouts of mobility reflect volitional transitions between functional activities and are

reported ambulation data in that most bouts were short in

Wheelchair users are in movement only about 10% of the time up in their chairs.

Involved in other functional activities for much of the other 90% of the time.

(Sonenblum, Sprigle, & Lopez, 2012)

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Individuals who use wheelchairs do much more than propel from wheelchair

• For many, it is the position from which they perform all ADLs





ROLE OF THE WHEELCHAIR FOR THE USER

How Do We Approach the Prescription Process?

- 1. Body Function & Structure
- 2. Activity & Participation
- 3. Environmental & Personal Factors



Body Function & Structure

COGNITIVE IMPAIRMENT SKIN INTEGRITY RANGEPERCEPTION OF POSTURAL ASYMMETRIES OF DISEASE **MOTION SECONDURANCE SECONDURANCE SECONDURANCE** PAIN



Activity & Participation

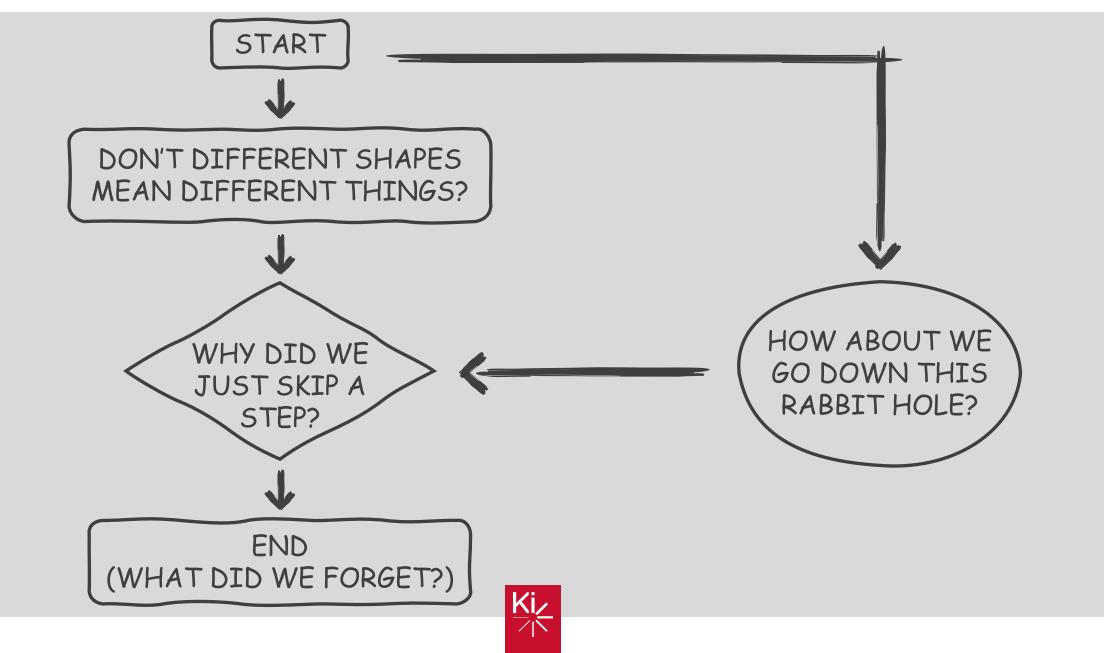
MEAL PREPARATION Essential ISFER DUTIES BATHING DRESSING YMENT



Environmental & Personal Factors

TRANSPORTATION SUPPORT HONSHIPS HON **TECHNOLOGY** CCESSIBILITY ACCESS AND **COMMUNITY ACCESSIBILITY**





Return to Evidence-based Practice



Establish a Foundation Posture

We cannot consider

- functional activities
- wheelchair propulsion

until postural stability has been addressed





FOUNDATION POSTURE

Optimal Static Posture



FOUNDATION POSTURE

Optimal Static Posture





OPTIMAL STATIC POSTURE

An individual's neutral alignment is dependent on:

- Range of motion
- Strength
- Muscle imbalances
- Endurance
- Muscle tone and response
- Lifestyle/habits



STATIC POSTURAL CONTROL

In order to maintain static postural control, an individual needs to be able to maintain a position of balance



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Dynamic posture is person's alignment during activity





Dynamic posture is person's alignment during activity

Requires ability to maintain Center of Gravity (CG) over a constantly changing Base of Support (BoS)





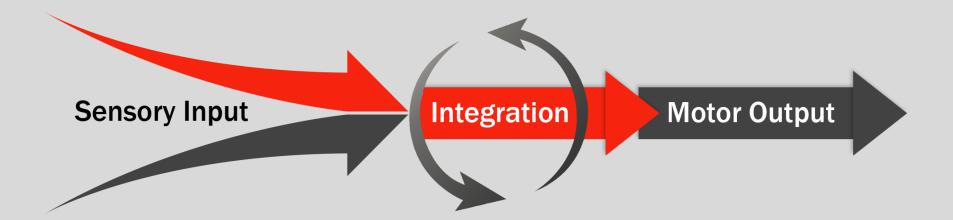
Dynamic posture is person's alignment during activity

For an individual who uses a wheelchair, requires maintaining a changing **CG** over a fixed **BoS**





Dynamic postural control requires integration of sensory input for motor output

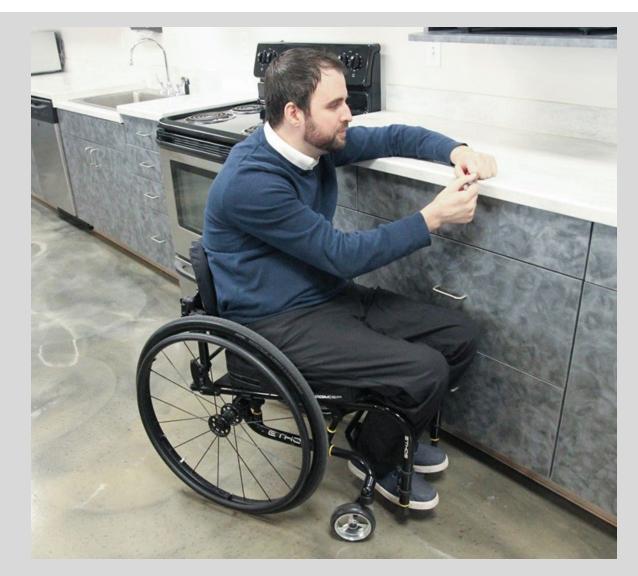




Dynamic postural control requires integration of sensory input for motor output













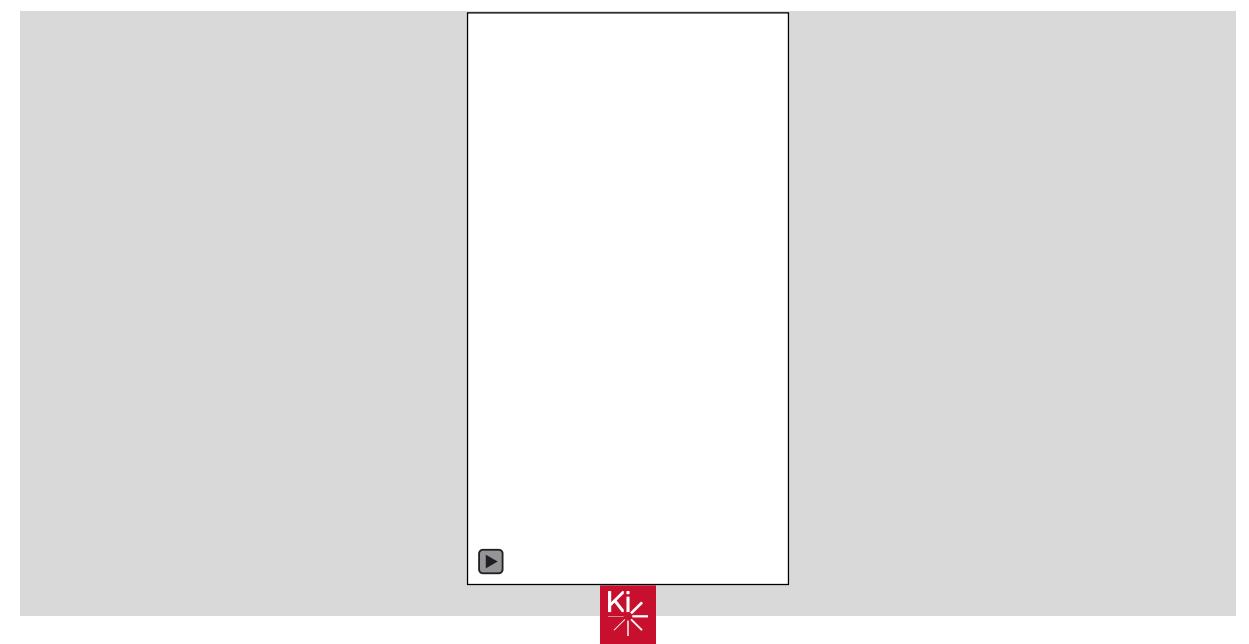








DYNAMIC POSTURAL CONTROL



DYNAMIC POSTURAL CONTROL

Put stability of posture to the test with dynamic functional activities

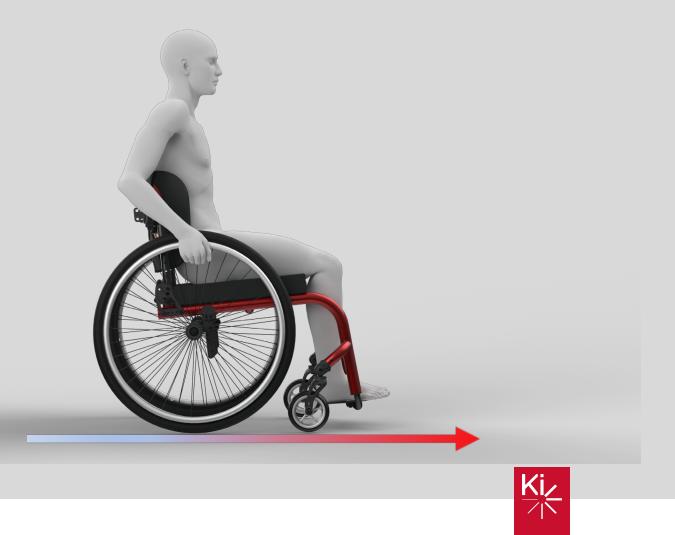
• Activities chosen by user





DYNAMIC POSTURAL CONTROL

Then we can put stability of posture to the test during propulsion



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The influen on wheelch

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Jui-Te Lin & Steph

Advances in Mai Techn

Carmen P. DiGiovine, Alicia M. k

ine manual wneeschair has undergone much advance afticle is to provide an overview of the most significant a advance are new availade in the clinical cations are ances to provide an overview or the instances of thing and advances are now available in the clinical setting and devices clinicians environment funders courses and an alvances are now available in the clinical setting and accions, clinicians, engineers, funding sources, and, m and and accions is being selected. Key words: a wheel-that wheel-that is being selected. manual wneekriair is being selecte wheekhair, wheekhair propulsion

The manual wheelchair is an incredibly intriguing and important piece of technology. For individuals who rely on manual wheelchairs for mobility within the community, these wheelchairs can be the community, mease where the end of the two of tw being their greatest limiting factor! To the untrained observer, the manual wheelchair has not changed significantly over the past 60 nasing change usignificantly over the past of years since the advent of the first folding rears anne un auven or un unst rouning frame manual wheelchair. However, the trante mattuat wheelchair, rowever, the manual wheelchair, especially ultralight wheelchairs, are technological marvels of wincentiants, are recumoused marves or sophistication. The advances include dereases in weight and size (form factor) of the frame and all components, increased name and an components, mereased adjustability to fit the individual, reduction in aujusaumny as in the maximum, remension in vibrations transmitted to the user, attention to violations transmuteu to the user, autention to details such as transportability and transpoructains such as transportantity and transpor-tation, improved propulsion methods, and Listo increased func-

Disability and Rehabilitation: Assistive Technology Shoulder Biomechanics During the Push Phas Propulsion: A Multisite Study of Persons Wi Jennifer L. Collinger, BS, Michael L. Boninger, MD, Alicia M. Koontz, PhD, Sue Ann Sisto, PT, MA, PhD, Michelle L. Tolerico, MS, Rory A. Cooper, PhI ABSTRACT. Collinger II., Boninger ML. Kooniz AM, Price R. Sisto SA, Tolerico ML. Cooper RA. Shoulder biome chantisie study of persons with paraplegia. Arch Phys Med Rehabil 2008;89:667-76. Objectives: To present a descriptive analysis and compari-ty of shoulder bioaster and binarrative Andrew automations Vectives: To present a descriptive analysis and compari-f shoulder kinetics and kinematics during wheelchair wind at multiple speeds (self-selected and stady-state member for a large memory of memory memory). propulsion at multiple speeds (self-selected and steady-state target speeds) for a large group of manual wheelchair users with naradieoia while also investigation the accurate of endowed target speeds) for a large group of manual wheelchair users with paraplegia while also investigating the effect of pain and subject demonstration on promotion Rehabilitation Case series. Three biomechanics laboratories at research PEOPLE witti parapregia witte and investigati subject demographics on propulsion. institutions. Participants: Volunteer sample of 61 persons with paraplemobility, W gia who use a manual wheelchair for mobility. Intervention: Subjects propelled their own wheelchairs on a promotementer at a remote (calf content of 0 content of 2 generic) where force to the Participants: Volunier sample of 01 persons gia who use a manual wheelchair for mobility. the joints o vention: Subjects projetted their own wheelchairs on a meter at 3 speeds (self-selected, 0.9m/s, 1.8m/s) while and standard and a sum encoded. wheelchair shoulder) kinclic and kinematic data were recorded. Main Outcome Measures: Differences in demographics tween sites, correlations between subject characteristics. International demographics and biomechanics between netoynamomener at 3 specus (sci1-secored, 0.3 kinetic and kinematic data were recorded. bearing. users rep manual 73%.7 Man sons with and without pain. Incar regression using subject characteristics to predict shoulder homechanics, comparison tanics between speed conditions. Significant increases in shoulder joint loading with wheek Results: Significant increases in shoulder joint loading with increased propulsion velocity were observed. Resultant force increased from 54.4±13.5N models were observed for the start 75.7±20.7N at 1.8m/8 (P=2.001). Body weight was the primary demographic variable that affected shoulder forces, whereas Cause this i pulsi 75.7 \pm 20.7N at 1.8m/s (P<.001). Body weight was the primary demographic variable that affected shoulder forces, whereas Rehat Boninger, MD, Human Engli ser, mil, Human Engin System, 7180 Highland A Pittsburgh Health Care S boningertäpitt.edu

PA 15206, e-mail: 0003-999308/8904-00308534.000 doi:10.1016/j.upmr.2007.04

Vice Chair, Department of Physical Medicine rice cnair, argummen of enjoyeen meaning and professor, Departments remainmann, and rrojessor, izepariments o Bioengineering and Rehabilitation Science and Tech-Bioensineering and Rehabilitation Science and Tech-nology. University of Pittsburgh: and Executive Direc-tor, Center for Assistive Technology of University Production & Interface Production Parameterization tor, Center for Assistive Technology of University Pittsburgh Medical Center, Pittsburgh, Pennsylvania.

CLINICAL PRACTICE GUIDELINE

Spinal Cord Medicine

Preservation of Upper Limb Function Following Spinal Cord Injury:

A Clinical Practice Guideline for Health-Care Professionals



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This guideline has been prepared based on the scientific and professional information available in 2004. Users of this guideline should periodically review this material to ensure that the advice herein is consistent with current reasonable clinical practice.

April 2005



OPTIMIZING THE WHEELCHAIR SETUP

Setup Factors

VERTICAL AXLE VERTICAL HORZONALANGLE POSITION



Influences two important aspects of wheelchair mobility

- Stability
- Propulsion efficiency



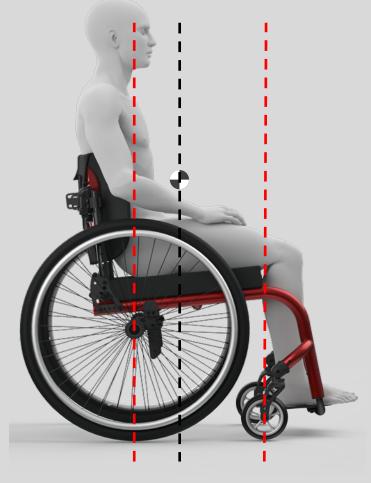
(Medola, 2014)



Center of Gravity (CG) Location vs. Mass Distribution

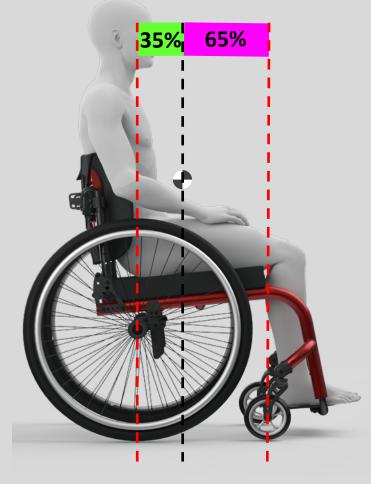
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CG Location in Wheelbase



Center of Gravity (CG) Location vs. Mass Distribution

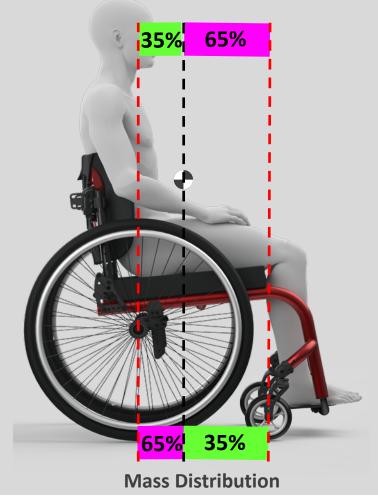
CG Location in Wheelbase





Center of Gravity (CG) Location vs. Mass Distribution

CG Location in Wheelbase





More rearward drive wheel position

- Decreases system mass over drive wheels
- Improves rearward chair stability
- Increases rolling resistance
- Decreases user access to drive wheel

(Gorce, 2012, Boninger, 2005, Freixes, 2010, PVA, 2007, Mulroy, 2005, Brubaker, 1986, Slowik et al., 2013)



Mass Distribution

55%

45%

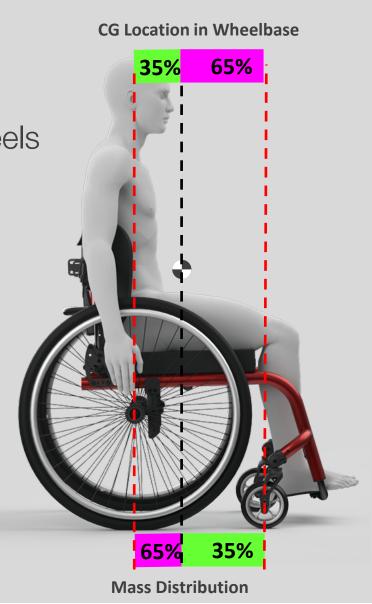
CG Location in Wheelbase

45%

55%

More forward drive wheel position

- Increases system mass over the drive wheels
- Decreases rearward chair stability
- Decreasing rolling resistance
- Increases user access to drive wheel



May need to prioritize stability for some users





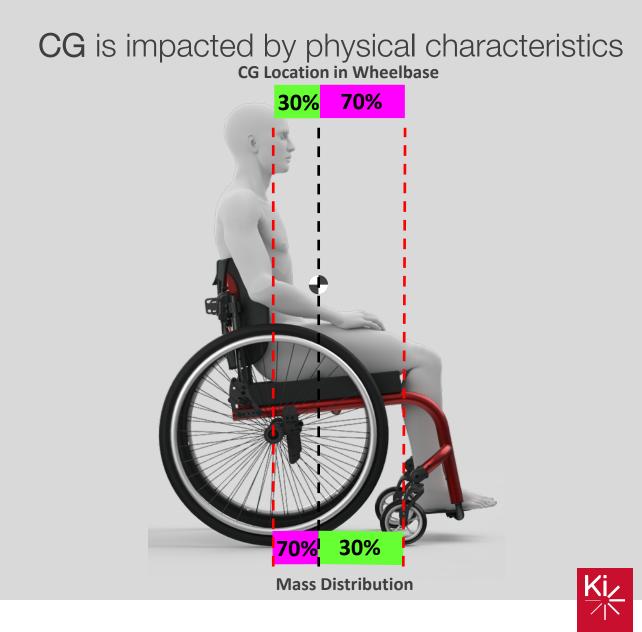


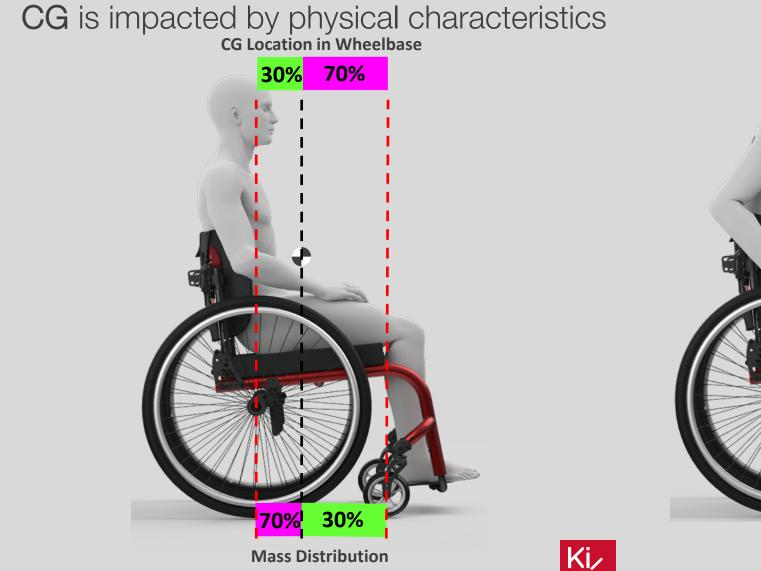
For others, you may need to prioritize agility concurrent with their skill level

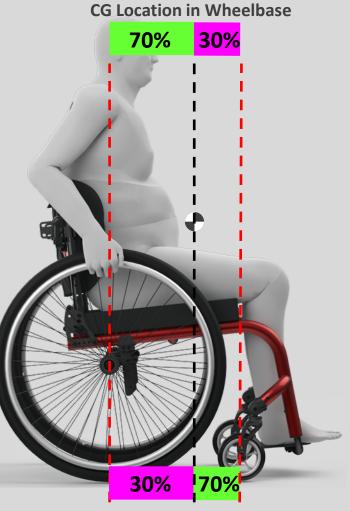




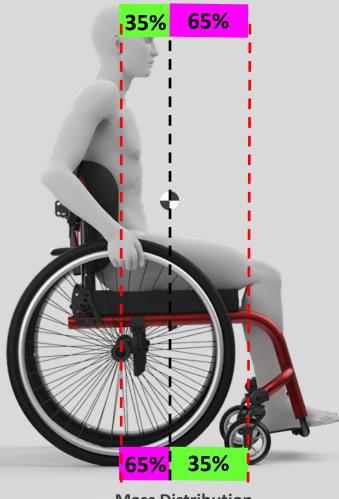






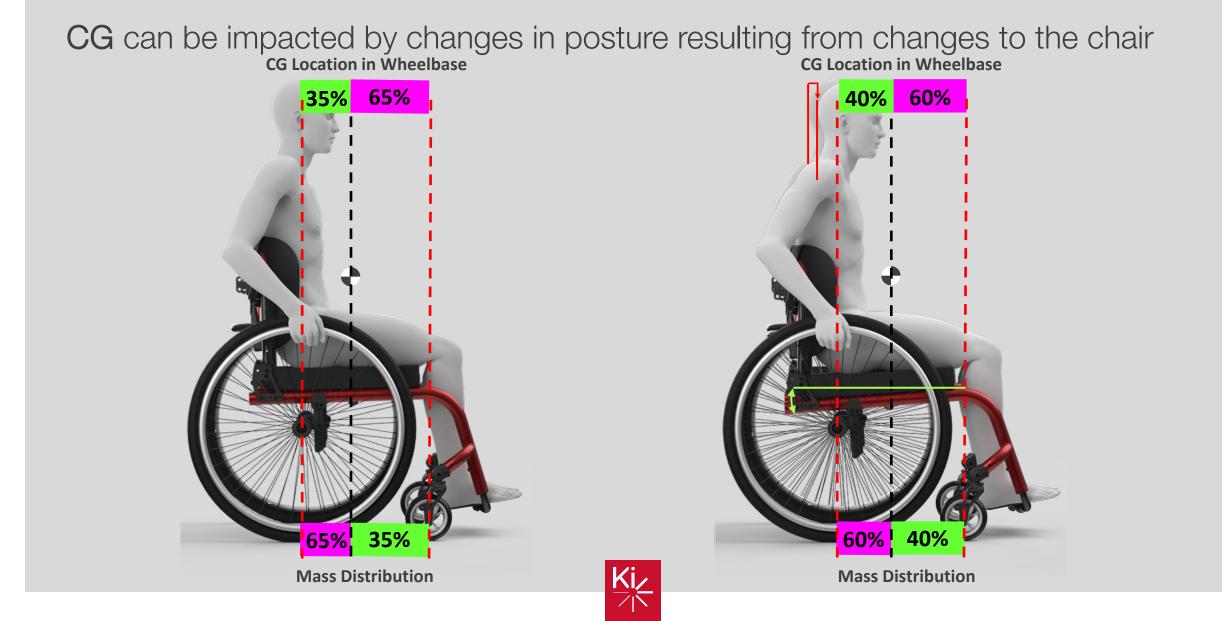


CG can be impacted by changes in posture resulting from changes to the chair CG Location in Wheelbase



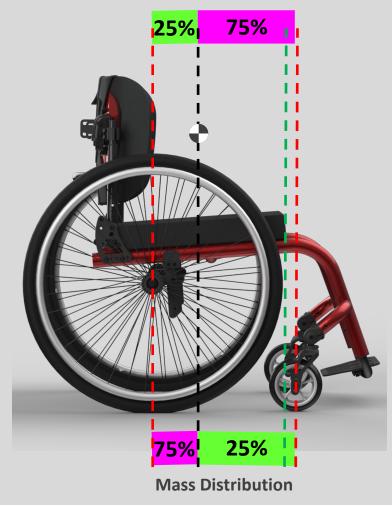
Mass Distribution





CG can be impacted by frame length

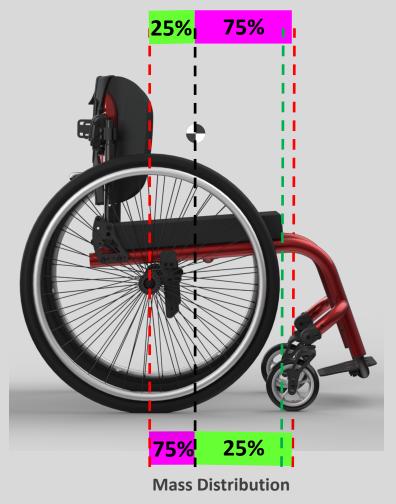
CG location in Wheelbase



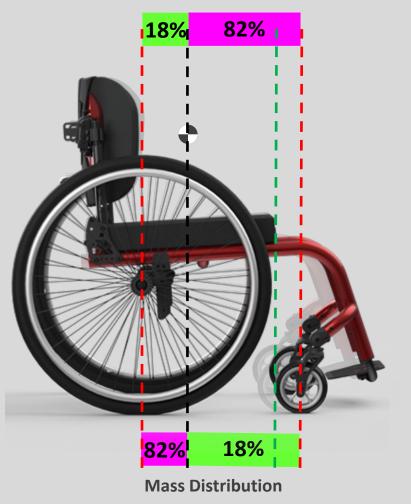


CG can be impacted by frame length

CG location in Wheelbase



CG location in Wheelbase



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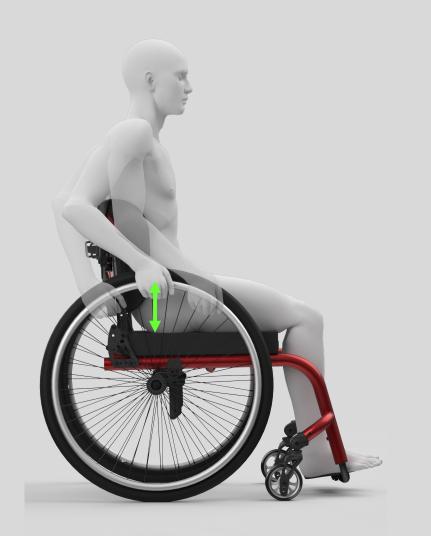
Vertical axle position impacts

- Stability
- Propulsion efficiency





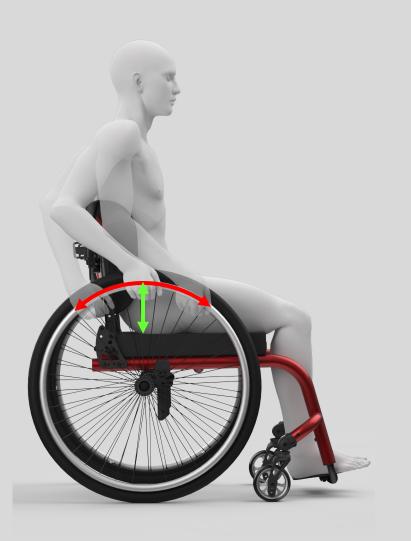
Rear seat height relative to the drive wheel





Rear seat height relative to the drive wheel

• Determines available wheel arc for propulsion

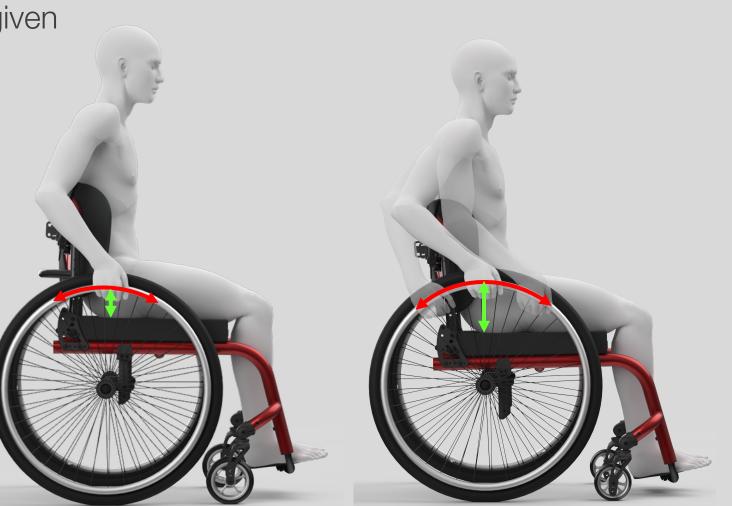


(Van der Woude, et al., 1989)



Higher seat heights for a given wheel diameter

• Reduces available wheel arc



(Van der Woude, et al., 1989)

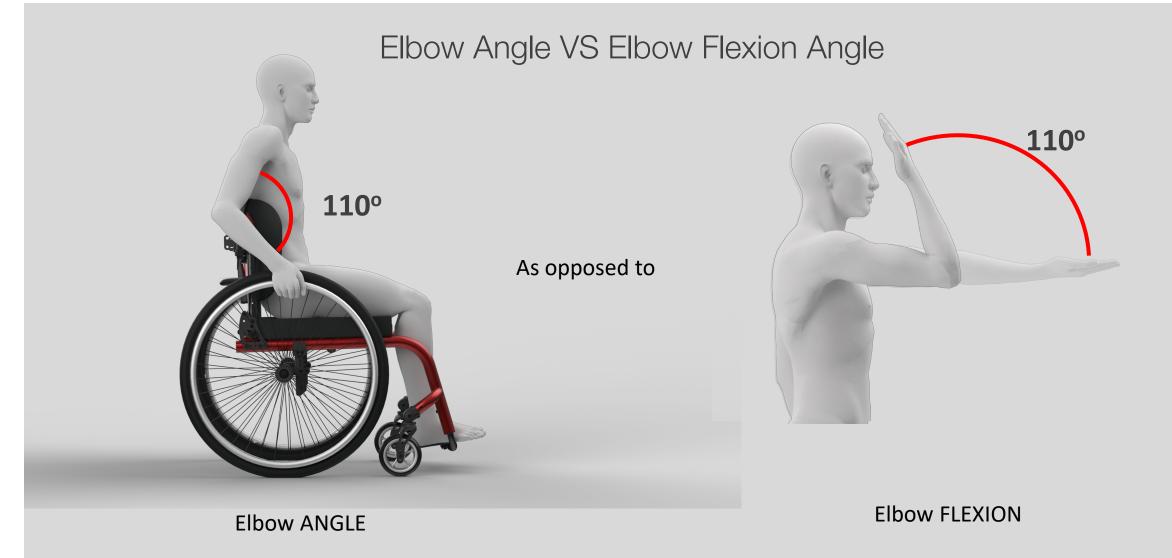


Higher seat heights for a given wheel diameter

- Shown to increase push frequency
- Increased potential
 for muscular fatigue

(Boninger, et al., 2000 & Boninger, et al., 2005)



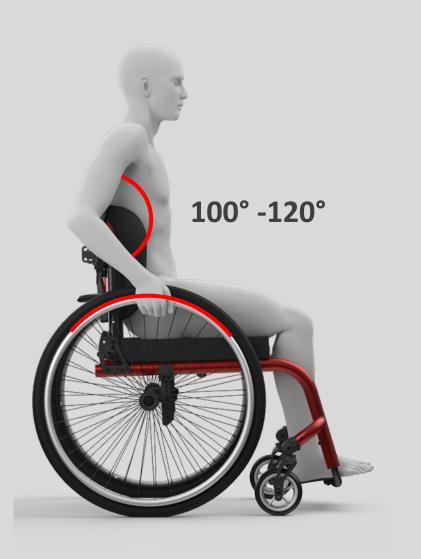


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100-120 degrees of elbow angle when hand is at top of handrim (12 o'clock)

- Maximizes user access to handrim throughout push stroke
- Places shoulder and elbow in most mechanically advantageous positions
- Protects the upper extremity by eliminating harmful ranges for shoulder and elbow

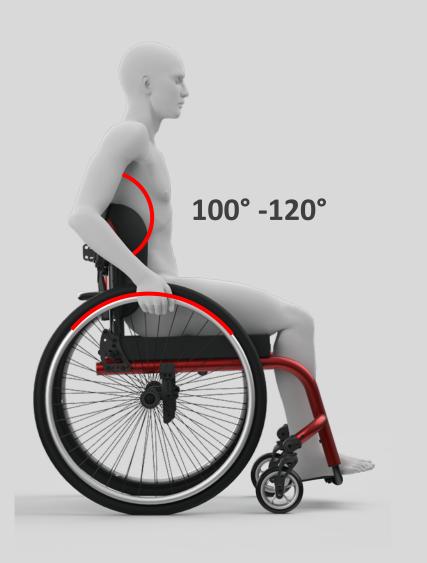
(Van der Woude, et al., 2009, Van Der Woude, et al., 1990, Mejis, et al., 1989)



100-120 degrees of elbow angle when hand is at top of handrim (12 o'clock)

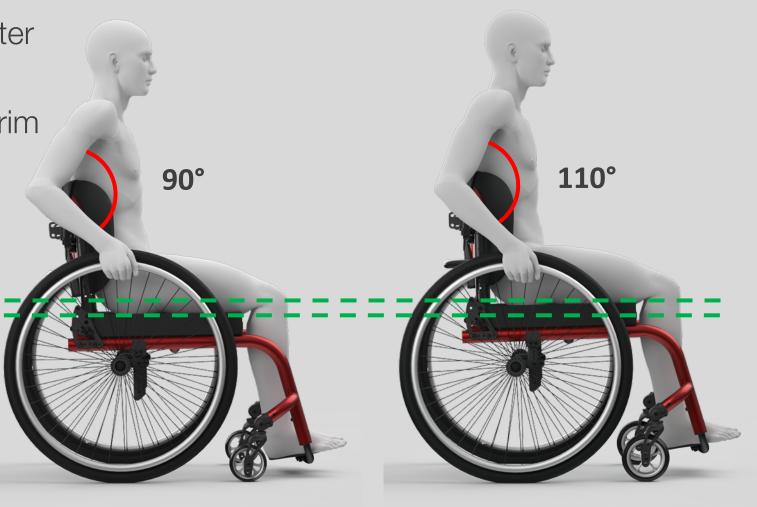
- Associated with improved propulsion efficiency
- Associated with decreased energy expenditure

(Van der Woude, et al., 2009, Van Der Woude, et al., 1990, Mejis, et al., 1989)



Lower seat heights for a given drive wheel diameter

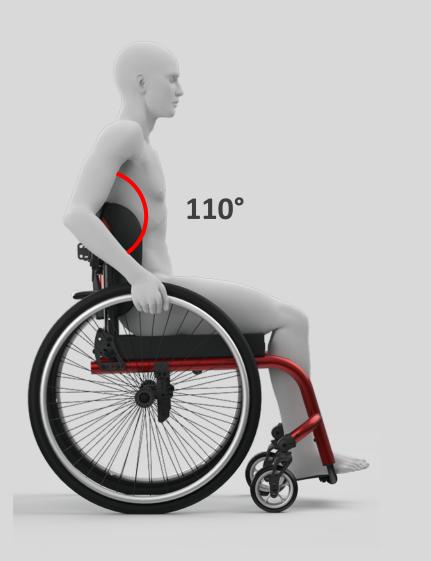
- Less efficient handrim forces
- Less efficient cardiorespiratory parameters



<u>Ki∠</u>

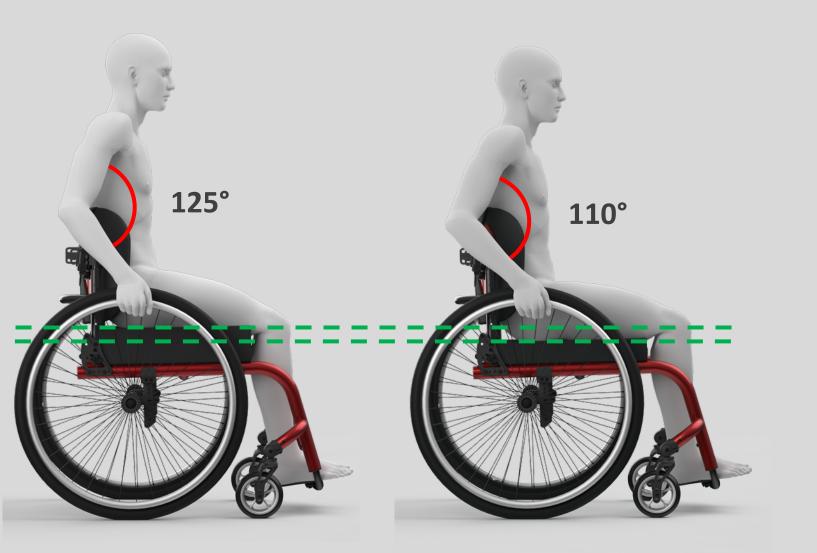
(Van der Woude, et al., 2009)

Vertical axle placement can be impacted by seat cushion height



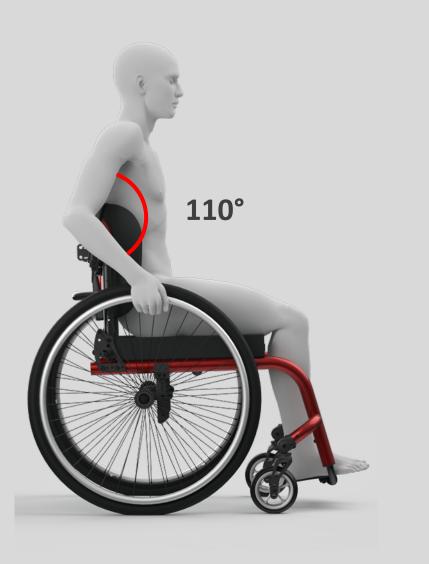


Vertical axle placement can be impacted by seat cushion height



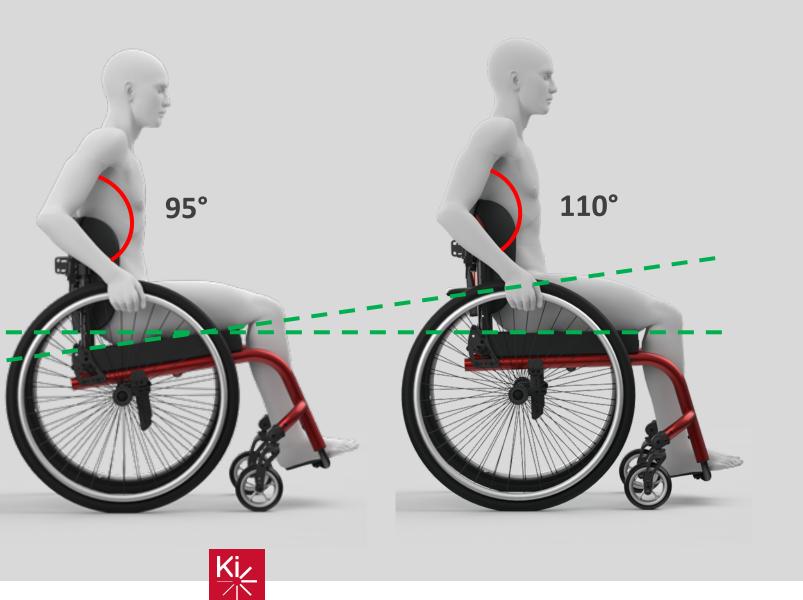


Vertical axle placement can be impacted by the need for seat slope

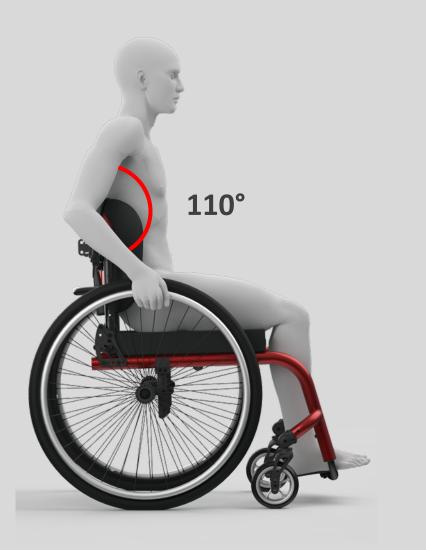




Vertical axle placement can be impacted by the need for seat slope

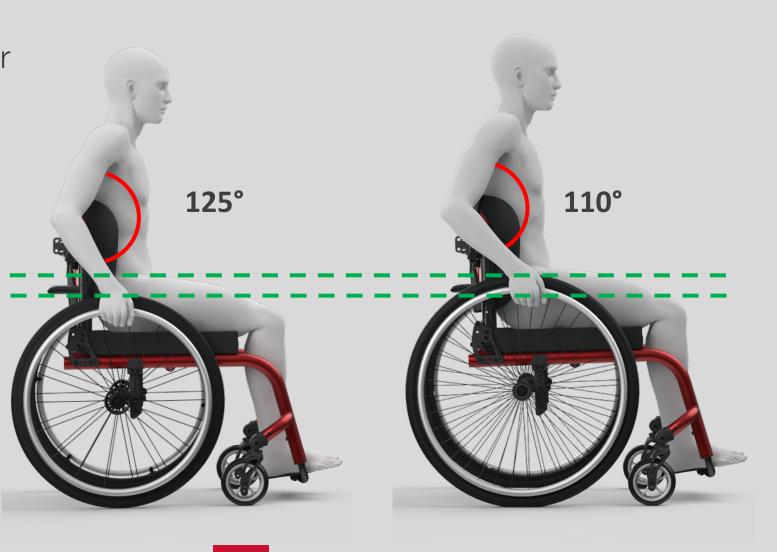


Vertical axle placement can be impacted by rear wheel diameter



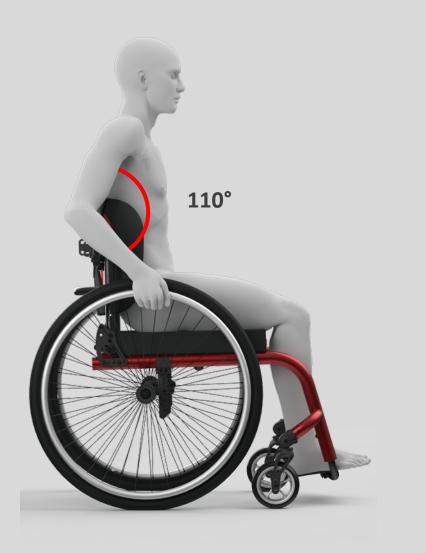


Vertical axle placement can be impacted by rear wheel diameter



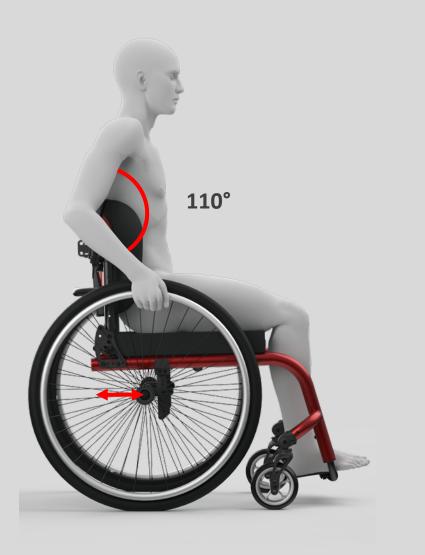


Elbow angle can be affected by other set up choices





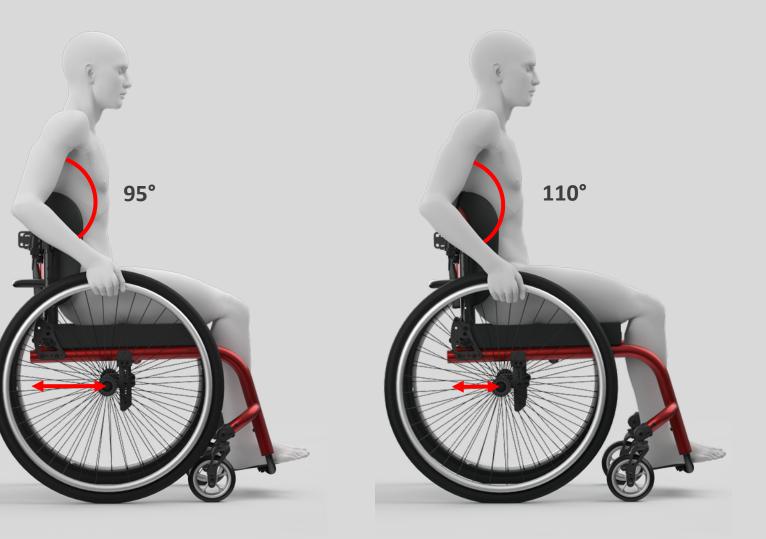
Horizontal axle placement can impact elbow angle





AXLE POSITION IN VERTICAL PLANE

Horizontal axle placement can impact elbow angle

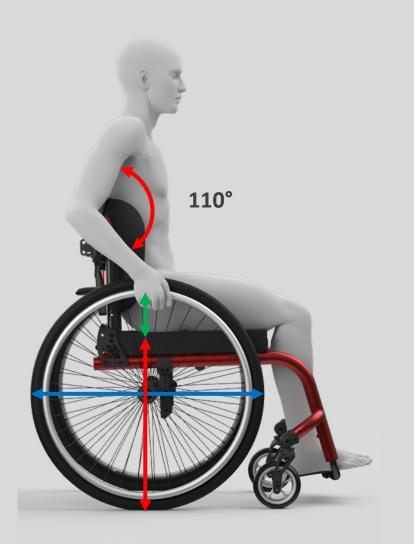




Formula for Wheel Size

- Measurements needed:
 - Seat to Palm (SP)
 - measured in the desired seated posture
 - with an elbow angle of 110°
 - Rear Seat Height (RSH)
 - Wheel Diameter (WD)

SP + RSH = WD







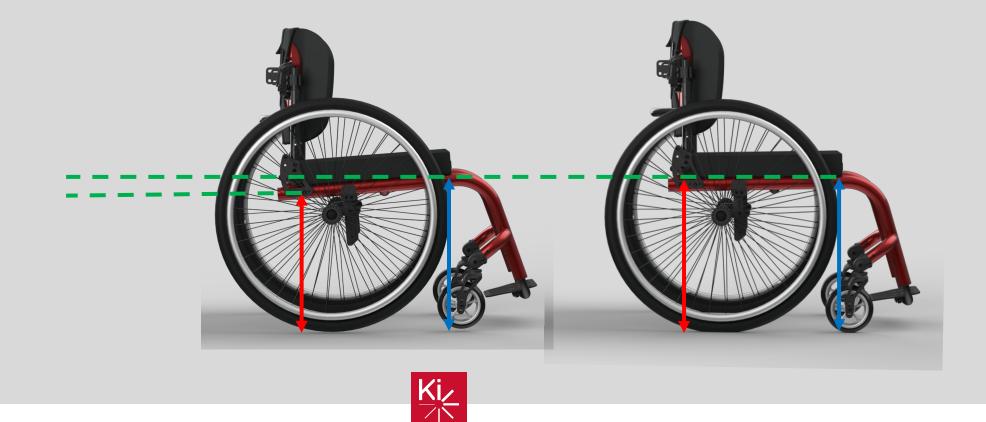
Often thought of as the difference between Front Seat Height and Rear Seat Height or "Dump"





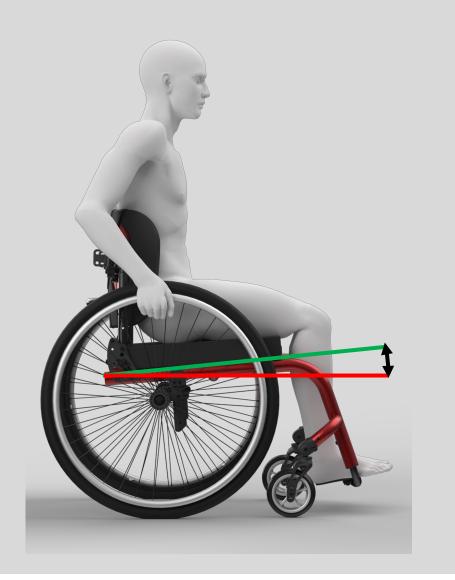


Often thought of as the difference between Front Seat Height and Rear Seat Height or "Dump"



Angle is the figure formed by two rays, sharing a common endpoint

• Seat Inclination relative to the Horizontal Plane



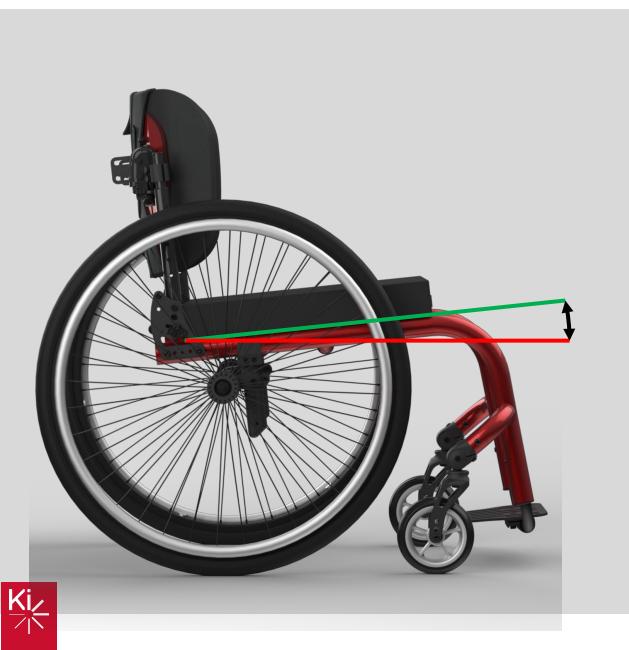


Formula for Seat Angle

- Measurements needed:
 - Front Seat Height (FSH)
 - Rear Seat Height (RSH)
 - Seat Depth (SD)
- FSH-RSH="Dump"
- Dump/SD =sine
- Inverse of sine converted to degrees = Seat Angle

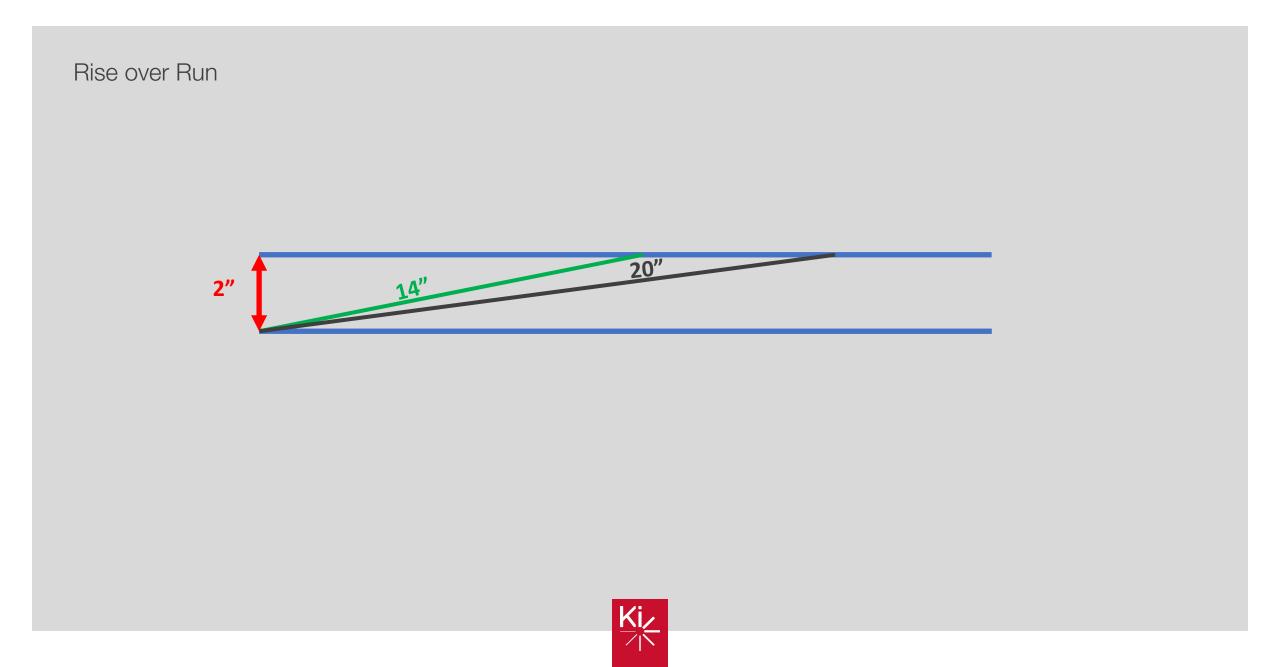


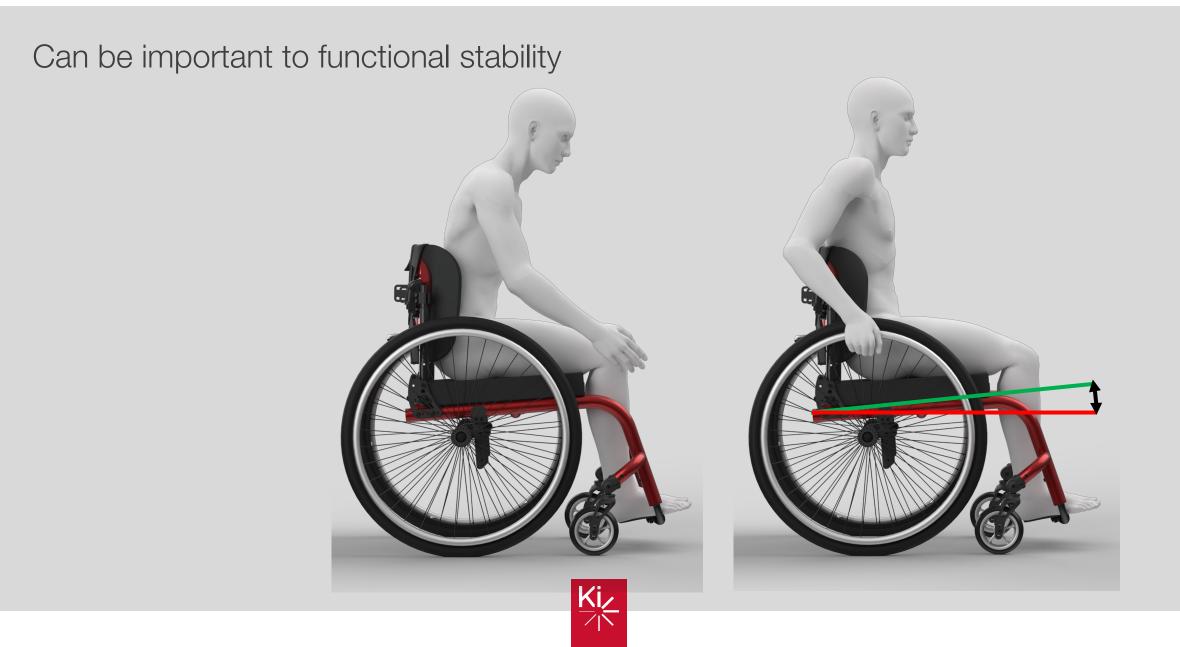
"Dump"	Seat Depth	Seat Angle
0	0	0°
2	14	8.2°
2	15	7.6°
2	16	7.1°
2	17	6.7°
2	18	6.4°
2	19	6°
2	20	5.7°
3	14	12.2°
3	15	11.4°
3	16	10.7°
3	17	10.1°
3	18	9.5°
3	19	9°
3	20	8.6°



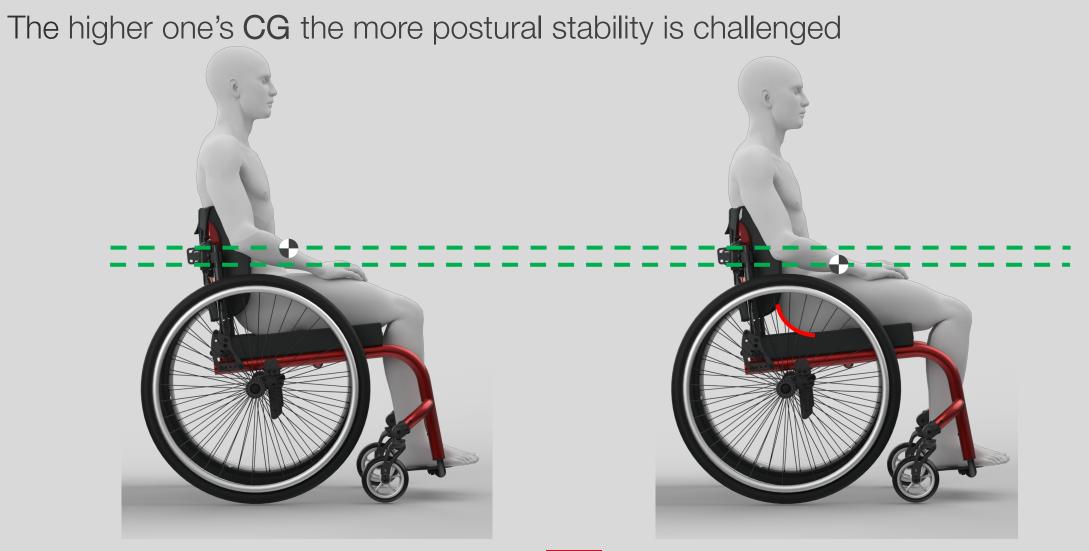






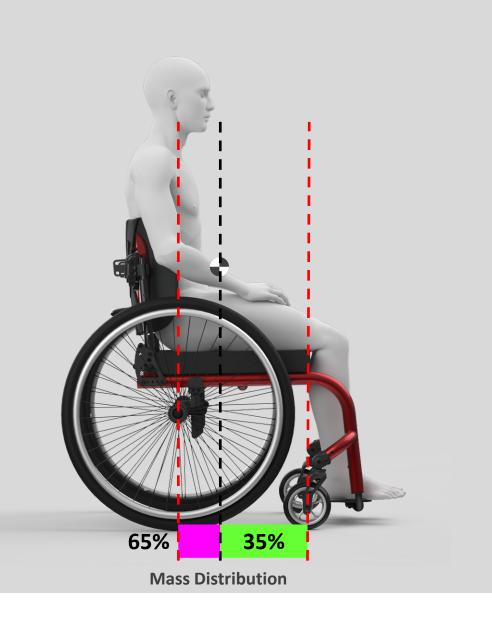






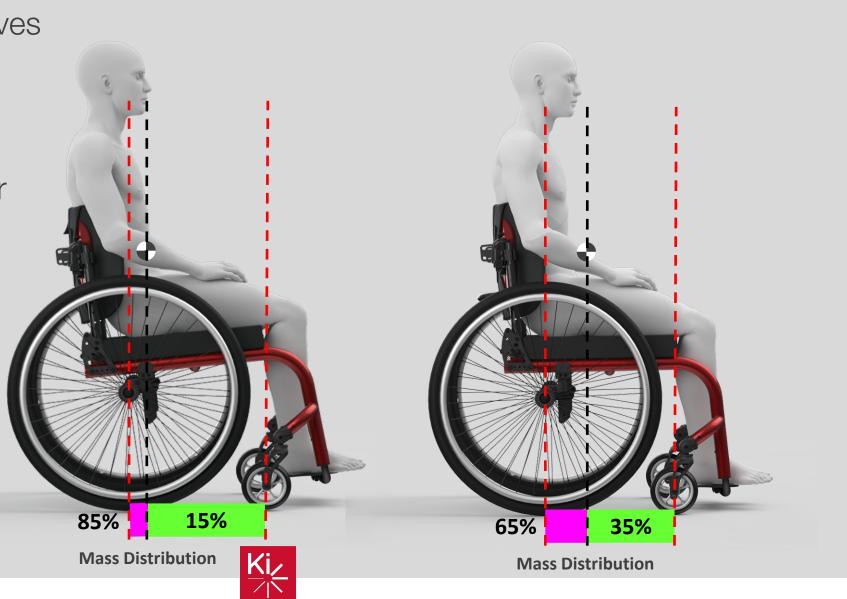


- Lowering CG improves seated stability
- Can impact weight distribution over rear wheels

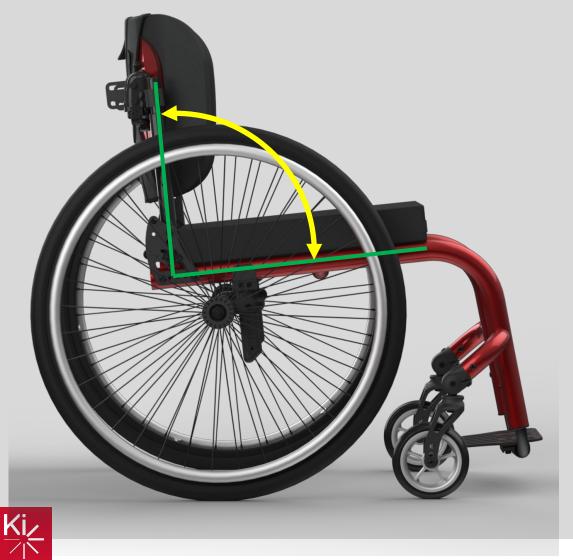


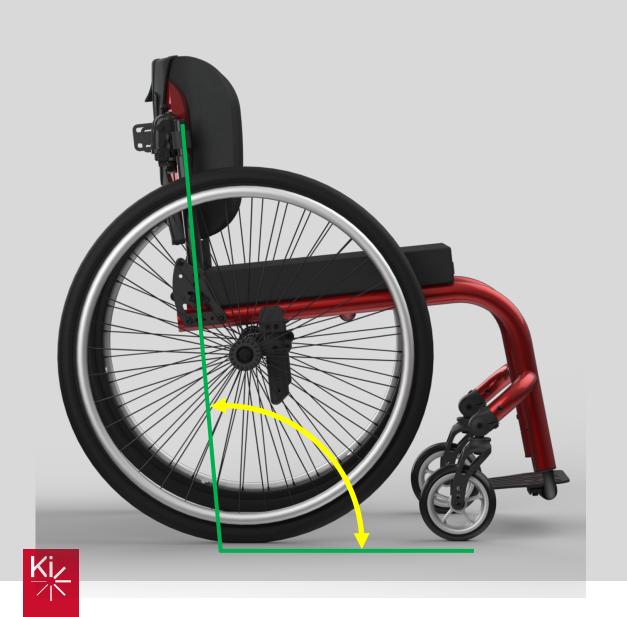
Ki/

- Lowering CG improves seated stability
- Can impact weight distribution over rear wheels



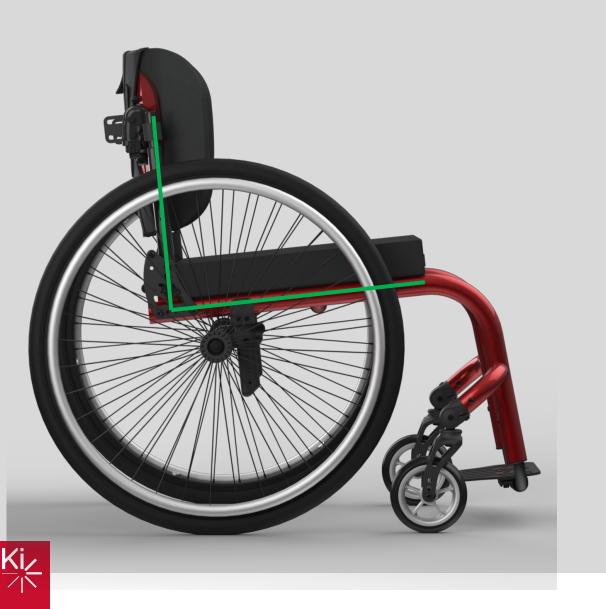
Measurement of back cane angle in relation to seat rail





Like seat angle, often used to facilitate

- Improved seated stability
- Functional use of upper extremities



- Can impact access to rear wheels for propulsion
- Can impact weight distribution over rear wheels







May be altered throughout "life of the chair"







May be altered throughout "life of the chair"

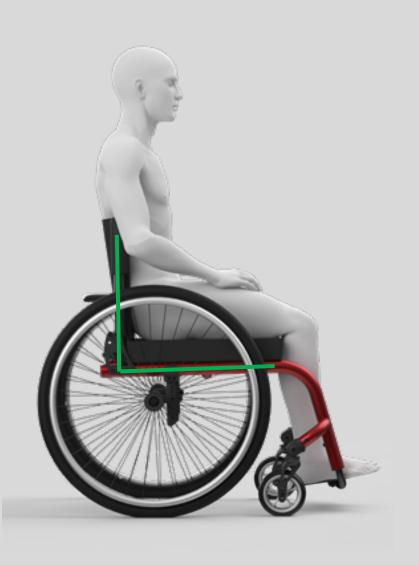






Back Upholstery

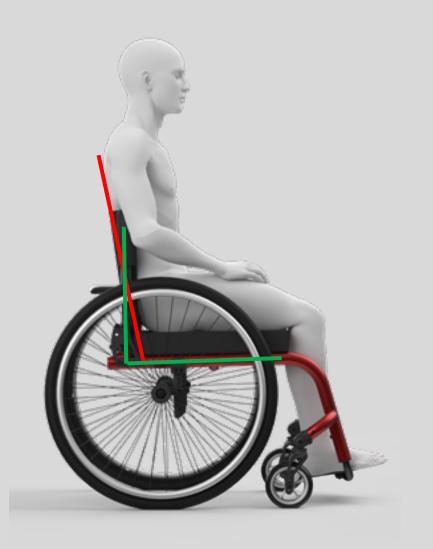
• Back Angle



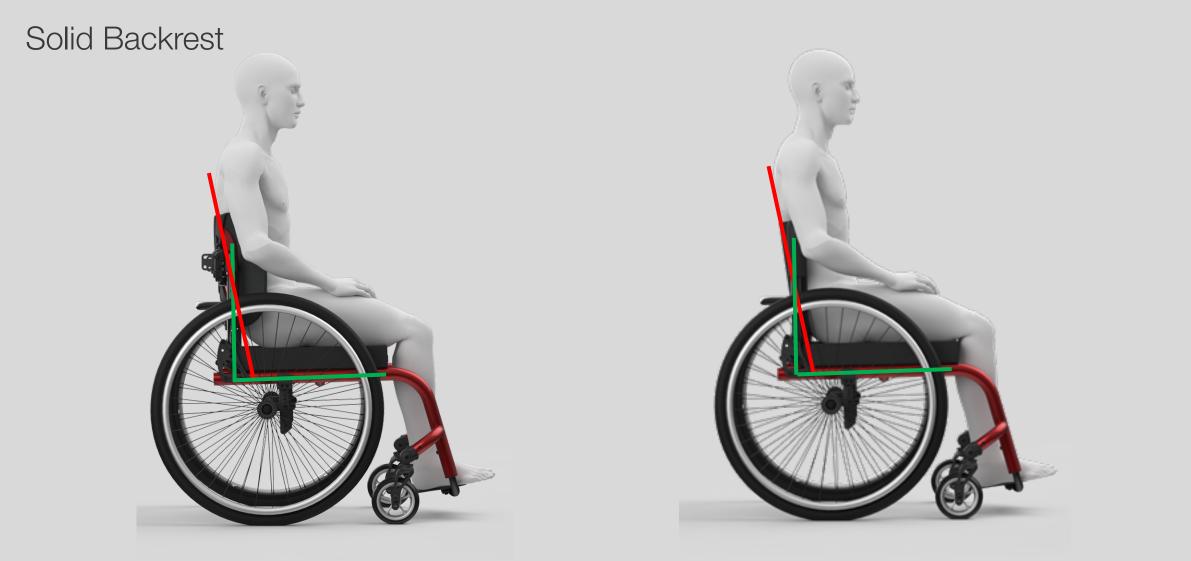


Back Upholstery

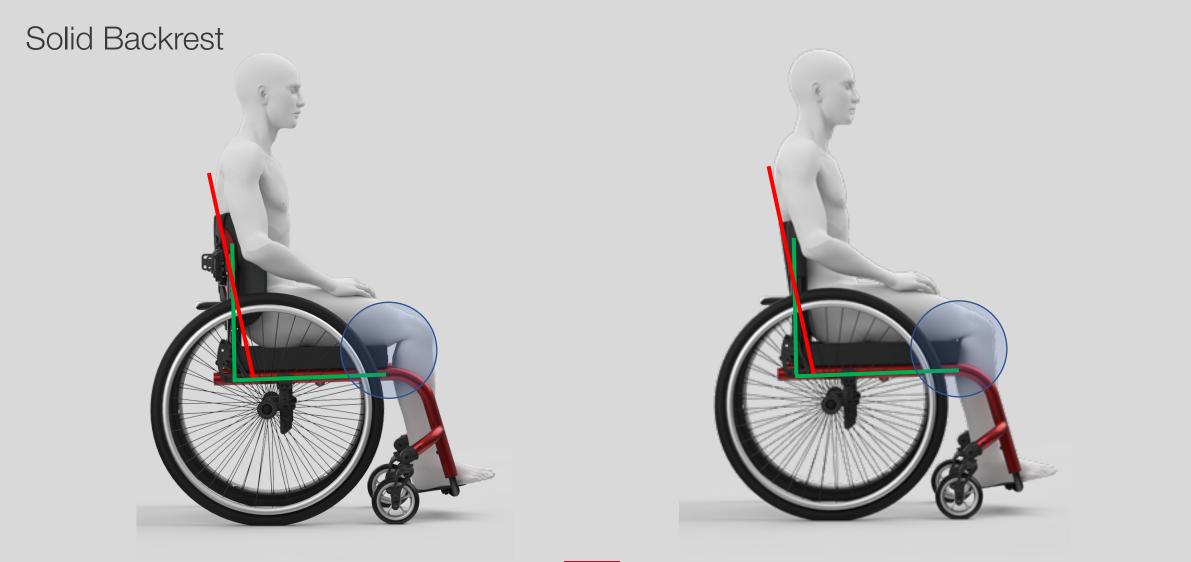
• Back Angle vs. Support Angle











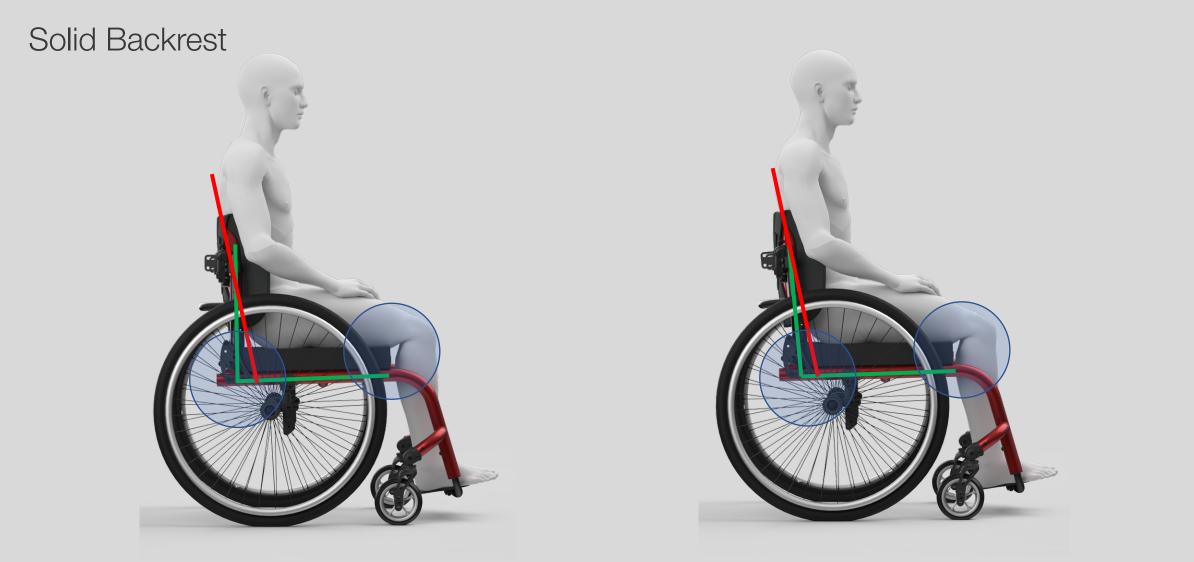




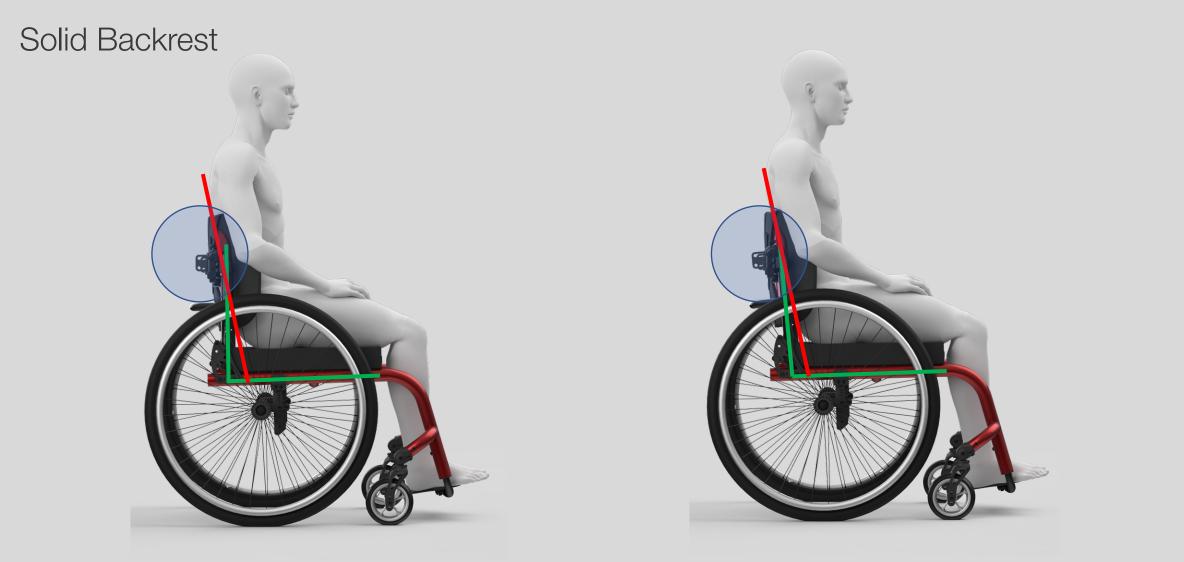














• Can impact postural stability

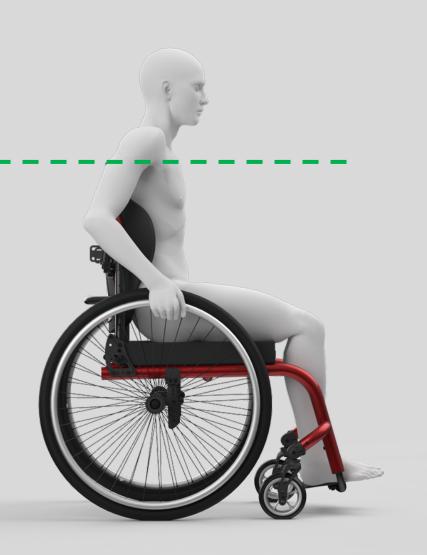
• Can impact upper extremity range of motion for function





Higher support

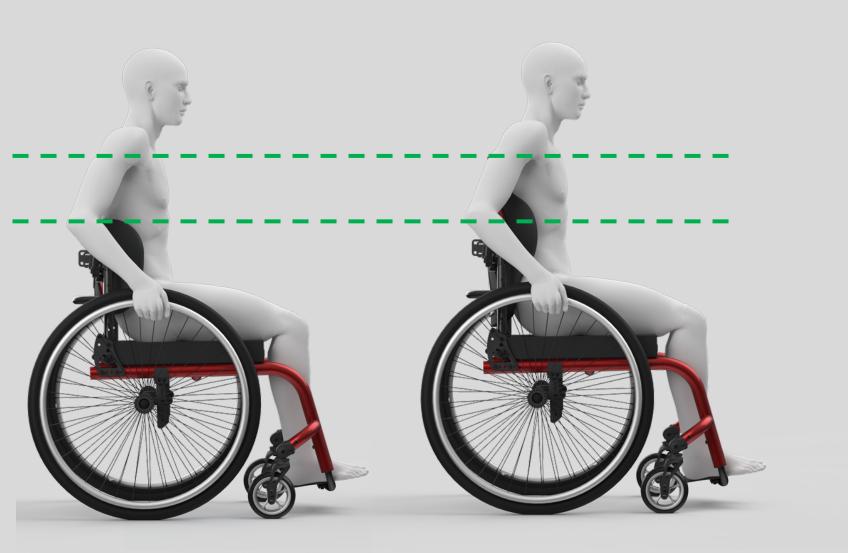
- Provides more posterior trunk stability
- May decrease shoulder extension range of motion





Lower support

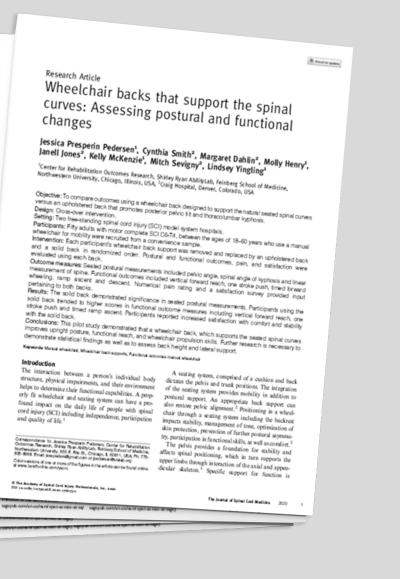
- Provides less posterior trunk stability
- May increase shoulder extension range of motion





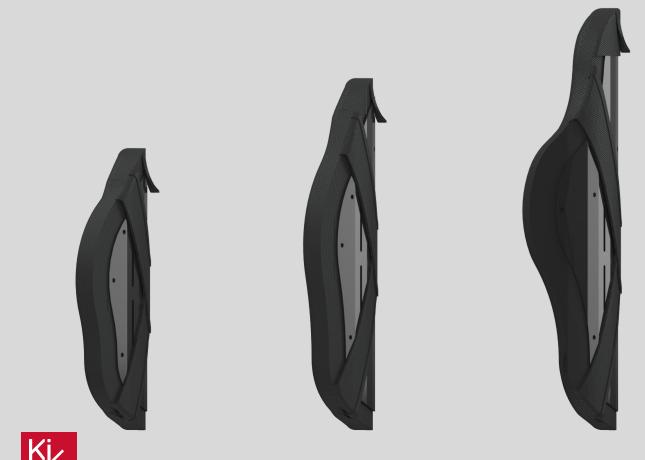
A pilot study on the impact of solid back support

- Higher vertical reach
- Longer one stroke push
- Faster 23 meter push
- Faster ramp ascent



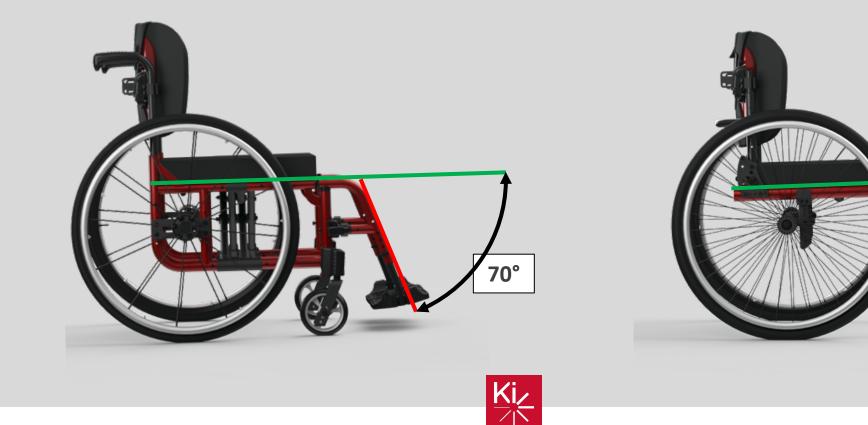
Lower backrest

- Greater shoulder range of motion
- Longer push stroke
- Greater push time
- Reduced push
 frequency
- No significant impact on handrim forces



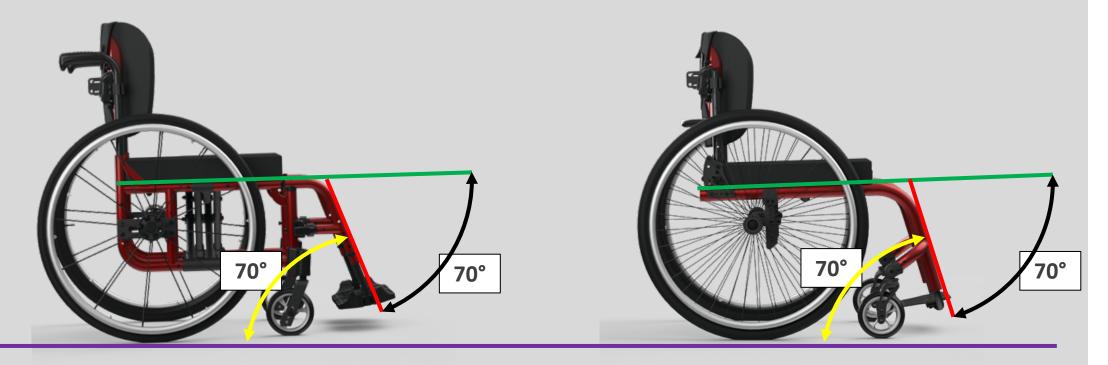
Yang et al., (2012)

Measurement of lower leg support angle



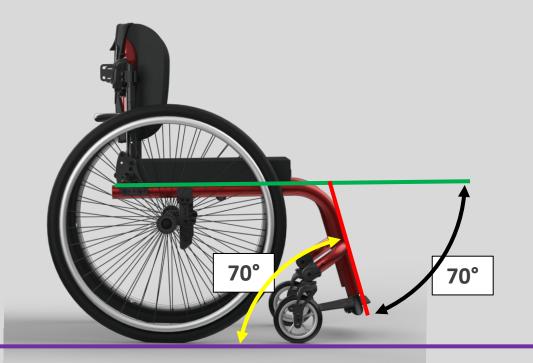
70°

Measurement of lower leg support angle



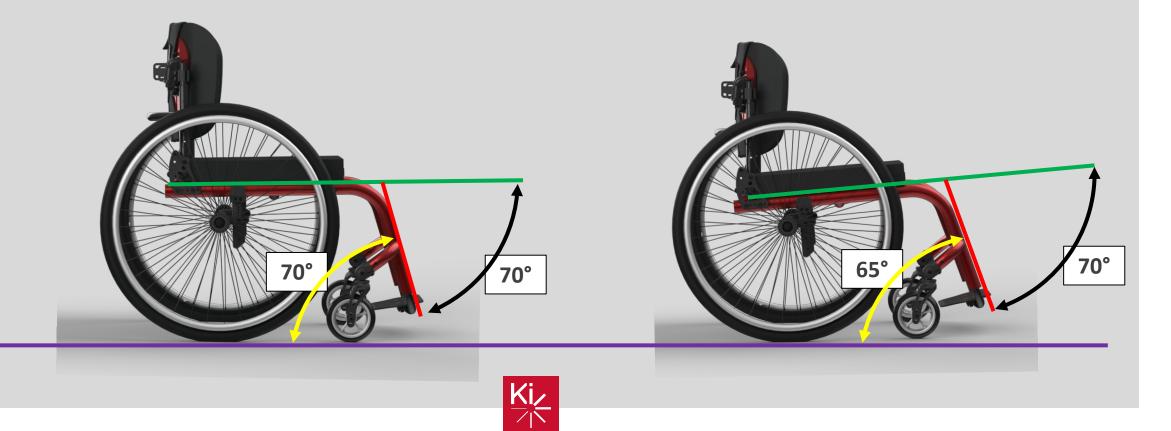


Measurement of lower leg support angle





Measurement of lower leg support angle



Considerations

- Hamstring length
- Range of motion (hip/knee/ankle)
- Spasticity/Tone
- Seated stability
- Maneuverability





PUTTING IT ALL TOGETHER

PUTTING IT ALL TOGETHER

A wheelchair needs to be set up for all the activities that a user performs from the device



A wheelchair needs to be set up for all the activities that a user performs from the device

It requires adjustability to optimize the setup for changes in functional ability and need



A wheelchair needs to be set up for all the activities that a user performs from the device

It requires adjustability to accommodate changes in functional ability and need

Adjustments to a single set up factor do not happen in isolation



A wheelchair needs to be set up for all the activities that a user performs from the device

It requires adjustability to accommodate changes in functional ability and need

Adjustments to a single set up factor do not happen in isolation

Using Evidence Based Practice provides a framework to plan for potential changes in wheelchair setup



Optimize the Wheelchair to Take Advantage of the Technology to Get Best Outcomes, Now and In the Future!



Questions

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